

INFONET Seminar Application Group  
Two-dimensional ultrasound detection with  
unfocused frequency-randomized signals

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# Outline

- Background
- Introduction
- Theory
- Simulation model
- Results
- Conclusion

# Background

General US imaging use bandwidth and frequency to determine image resolution

- High frequency → narrower beam → better resolution
- High frequency → higher beam attenuation → lack of deep imaging

Therefore present US technique turned to increasingly grows of frequency range.  
Current frequencies for medical imaging is 2-20 MHz

# Introduction

Technique should be turned from focused to unfocused to escape frequency grows

- For each element randomly selected individual frequencies, resulting signal is includes large bandwidth.
- Single point is used to record time history
- Reconstruction of ROI is performed from analysis of acquired signal from single element
- Process is repeated with different frequency patterns to increase performance of reconstruction
- Signal analysis consists of a Fourier-based approach

# Theory

- First emitter approximated as an array of simple sources radiating on unique frequency.
- Another approximation that we can describe pressure at any point in a homogeneous space given by

$$p_w(r, t) = -ic_0 k_0 \rho_0 S_w g_w(r_{s_w} | r_0), \quad (1)$$

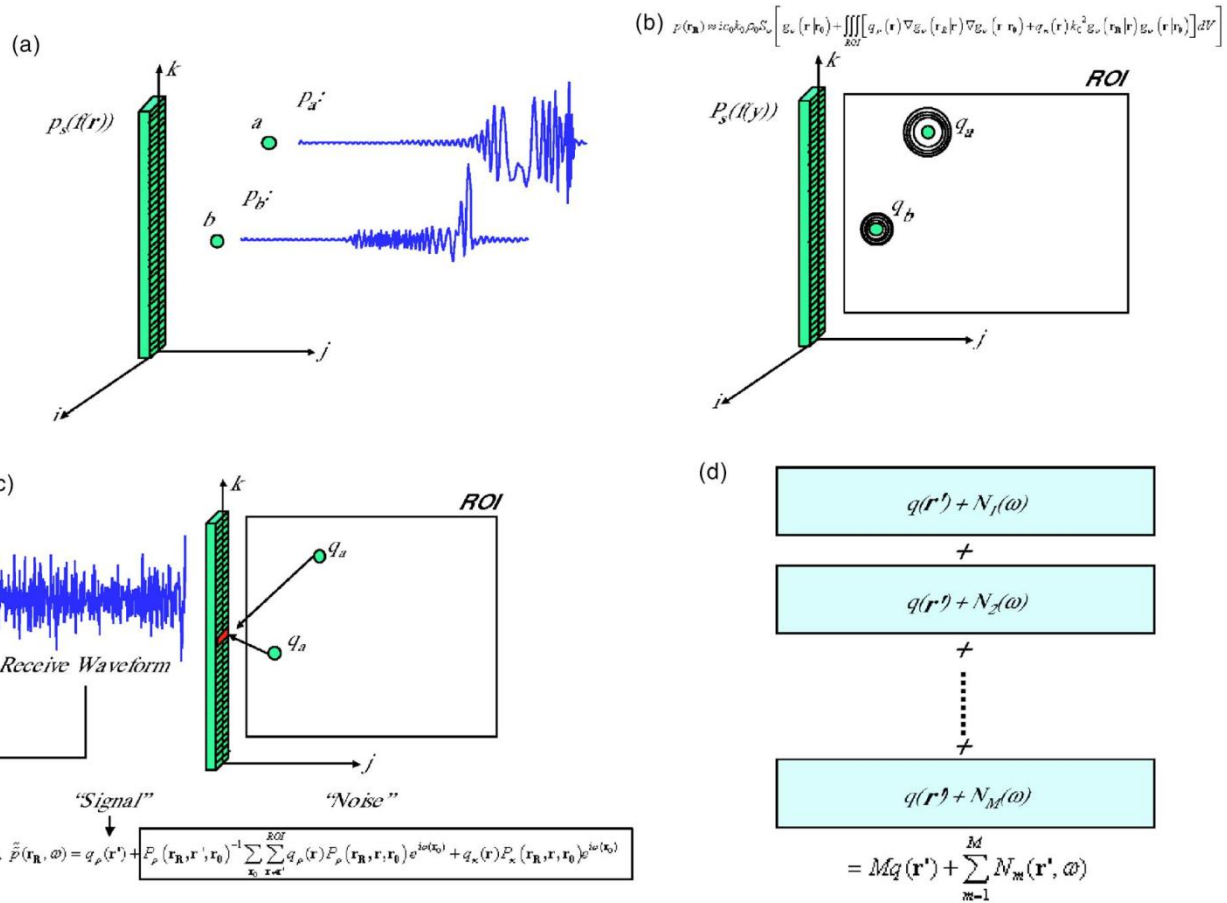
- Acoustic pressure for wave encounters a varying density may be described

$$\rho \nabla \left( \frac{1}{\rho} \nabla p_w \right) + \frac{w^2}{c^2} p_w = 0$$

- To improve SNR process with new random frequency distribution can be repeated M-times. With M signal strength will increase linearly while noise N will further randomized

$$\tilde{p}_M(r', w) = Mq(r') + \sum_{m=1}^M N_m(r', w)$$

# Theory



$$p(r_R, \omega) = q_p(r') + Pp(r_R, r', r_0)^{-1} \sum_{x_0} \sum_{r \in ROI} q_p(r) P_p(r_R, r, r_0) e^{i\omega(x_0)} + q_k(r) P_x(r_R, r, r_0) e^{i\omega(x_0)}$$

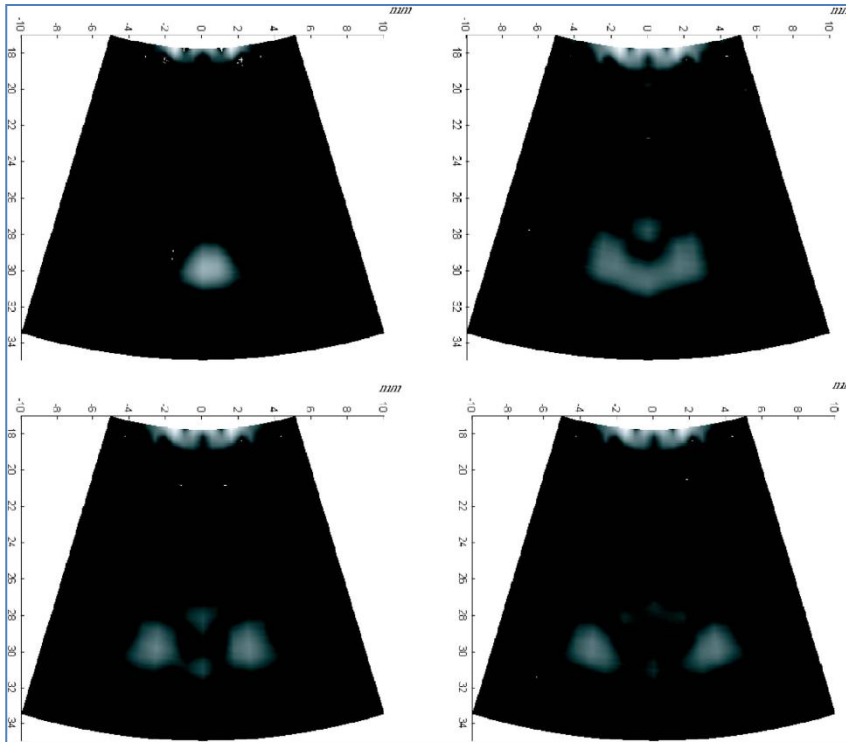
'Signal'

'Noise'

# Simulation model

- An operating frequency range between 0.1 – 1.25 MHz
- Simulated array is 40 mm in length and 10 mm in width
- Array segmented in to 202 linear sources with no kerf
- A linear distribution of 202 frequencies between 0.1-1.25 MHz with a frequency resolution of 5.7 kHz
- Each time randomly only one frequency assigned to element
- Also randomly single element selected to record signal
- Scattering field is placed within ROI
- Scattering signal at the receiver is discrete approximation of Eq. (10)

# Results

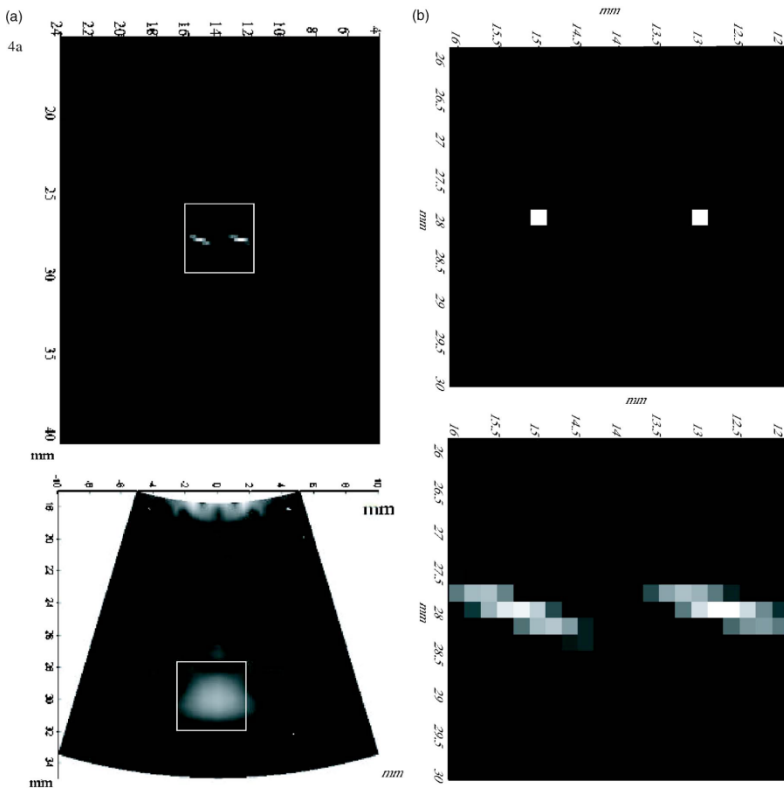


- Simulated B-scan via k-space projection algorithm using 200 ns resolution. Simulation was repeated for each of 21 scan directions
- ROI 40x40 mm
- Two objects with diameter 0.2mm was given sound speed of 3500 m/s
- Only on 8mm separation objects are clearly separated

Simulated B-scan images  $f_c=0.67\text{MHz}$ . Two wires with (diam=0.2mm) separated by a) 2mm, b) 4mm, c) 6mm, d) 8mm.



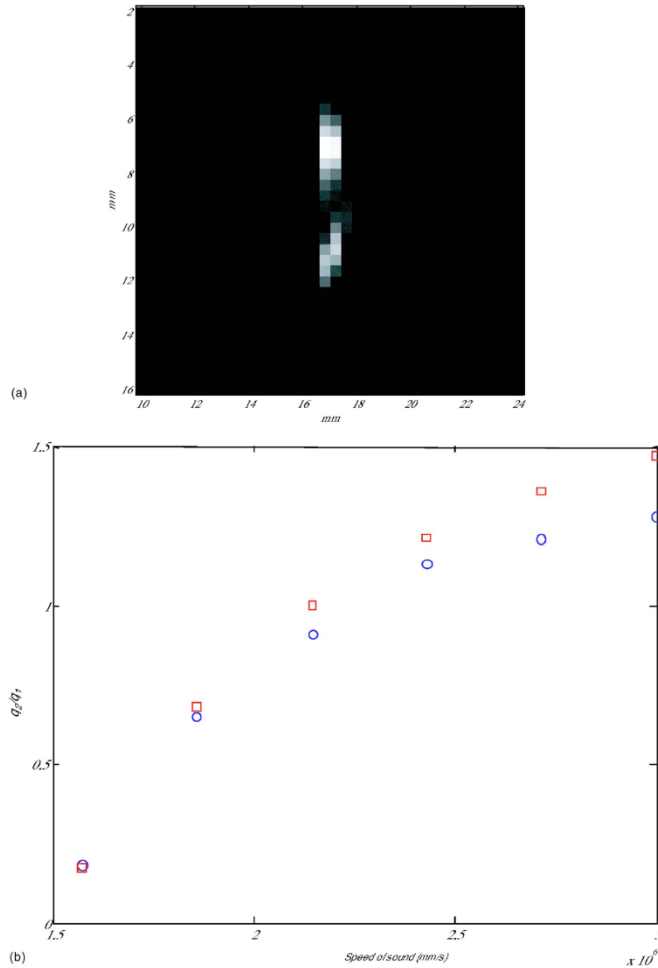
# Results



Comparison a) random frequencies (top)  
B-scan (bottom) b) more magnified view

- Comparing with B-scan method with randomized frequencies has better performance.
- Two objects can be imaged separately with 1.35 mm distance. Vertical 0.5mm
- Simulation was repeated with 15 randomized signals

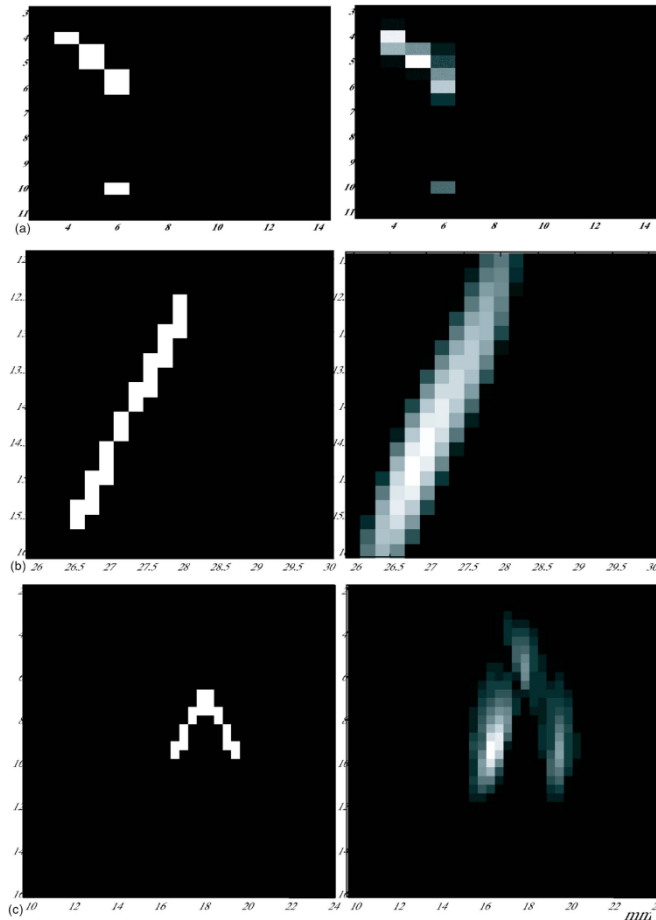
# Results



- Object placed 4 mm apart and 17 mm distance from transducer
- The plot shows trend of increased distortion with higher sound speed. Corresponding error ranged from 4.3% at 1857 m/s to 13% at 3000 m/s

Two reconstructed objects in the ROI with scattering strengths  $q_1=0.51$  and  $q_2=0.62$  (top) Scattering ratio of  $q_2/q_1$  is plotted as fn of frequencies (squares). Reconstructed values (cycles)

# Results



- Object placed 4 mm apart and 17 mm distance from transducer
- The plot shows trend of increased distortion with higher sound speed. Corresponding error ranged from 4.3% at 1857 m/s to 13% at 3000 m/s
- Three scatterers placed diagonally in 8x8 ROI and additional object 4 mm apart
- Object as an inverted “V” was situated 18 mm from the ultrasound source.

Simulation with multiple scatters (left column) and their reconstructions (right column). Distance from transducer a) 3-14 mm b) 10-24 mm c) 26-30 mm

# Conclusion

- Large variation in image field makes it possible to localize the position of targets
- In numeric investigation objects were better defined and more spatially localized
- Small objects, which can be hard to detect, and even hard to localize using present methods may be both detected and localized.
- Only single receive channel was used.

# Discussion

**Thank you**