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**39th Annual** International Conference of the IEEE Engineering in Medicine and Biology Society

International Convention Center (ICC), Jeju Island, Korea July 11 to 15, 2017

https://embc.embs.org/2017/

ThDT14-01: 16:10-17:10 Retinal Imaging (Poster Session)	Schaldach Room	ThDT14-07: 16:10-17-10 Ultrasound Imaging – Other Organs (Poster Session)
16:10 16:10	TEDT14.01.1	ThDT14-0
Retinal Vessel Segmentation using	110114-01.1	A New Synthetic Aperture recting Verification
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Tiwari, Ashwani Kumar (Wipro); Kanhangad, Vin	vek* (Indian Inst. of	Song, Hydrine Thomas Thomas Thomas
Tech. Indore); Pachon, Ram Bilas (Indian Inst. C	or rech. moore)	16:12-16:14
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0.40.40.40	THDT14-02 1	Song, Tai-Kyong (Sogang Oniversity)
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of Multiple Segmentation Algorithms	16 10 1643	Fermat's Spiral Scanning for 3D Plane Wave Ultrasound Imagin
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Technology); Klee, Sascha (Ilmenau Universit	ty of Technology)	ThDT14-
Address of the second second second second second	Ore, as an Incom	16:16-16:18 Reconstruct Ultrasonic Muscle Image to Analyze
ThDT14-03: 16:10-17:10	Schaldach Room	Muscle Density for Sarcopenia
JItrasound Imaging – Breast (Poster Session)		Song, Yu-Lin* (Asia University)
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Song, Ilseob (Sogang Univ.); Yoo, Yangmo* (	Sogang Univ.)	A New High Definition Multi-Planar Records and Method
A Design of the second s		Kim, Sung Chan (Sogang Univ.); Kang, Jinbum (Sogang Univ
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		Huang, Zhijie (Institute of Medical Information, School of
hDT14-05: 16:10-17:10	Schaldach Room	Biomedical Engineeri); Wang, Qing* (Southern Medical Univ.
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NI, Pavel (Gwangju Institute of Science and T Heung-No* (Gwangju Institute of Science and	d Tech. (GIST))	Ahn, Joongho (Pohang Univ. of Science and Technology);
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## Ultrasound Image Reconstruction using Compressive Sensing

Pavel S. Ni\*, and Heung-No. Lee, Gwangju Institute of Science and Technology

Original image inp

Abstract— In conventional sonography best resolvable resolution considered to be equal to two wavelengths. For ultrasound systems that operate at frequencies ranging from 3~15 MHz the finest resolvable resolution would be equal to 1~0.2 mm respectively. The diffraction limit determines resolution of conventional sonography systems. However, we show that it is possible to use interference of ultrasound waves to improve spatial resolution in medical ultrasound. Our work motivated by the fact that ultrasound fields can be accurately described using Huygens-Fresnel principle. Then, received by the array of elements RF signals can be considered as a superposition of reflected back, from inhomogeneity in the medium, ultrasound fields. We propose a new ultrasound imaging method that provides much greater details of small structures that usually cannot be observed in conventional sonography.

## I. METHOD

The underlying principle of sonography imaging based on array beamforming. Beamforming process used in transmit phase to focused ultrasound pulse and or in receiving phase to focus received ultrasound waves. In focused B-mode imaging transmit and receive beamforming used to acquire 2D ultrasound image. Likewise, in plane wave imaging only received beamforming used to focus ultrasound waves in post processing dynamically. Many different beamforming techniques have been proposed in past decades. However, ability to focus ultrasound waves have fundamental limit and imposes limit on the best achievable spatial resolution.

During transmission, all array elements simultaneously excited with code sequences. Then received at array signals can be modeled as

$$f_r(t) = \sum_{i}^{N_i} \sum_{j}^{N_j} \sum_{s}^{N_s} a_{i,j,r,s} h_s(t - t_{i,j,r,s}) .$$
(1)

where  $a_{i,j,r,s}$  is an amplitude of a point target at location

(i, j),  $h_s$  is shape of transmit ultrasound signals,  $t_{i,j,r,s}$  is round trip time of ultrasound echo's arriving to receiving element.

Ultrasound image can be reconstructed by following Compressive sensing framework as in

$$\min_{x} \|x\|_{w,1} + (1/\nu) \|Gx - f\|_{1} \quad s.t. \ x \ge 0$$
(2)

 $\label{eq:search} $$ Research supported the National Research Foundation of Korea (NRF) grant funded by the Korean government (NRF-2015R1A2A1A05001826). $$$ 

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Conventional B-mode

CS recovery image

Figure 1. Simulation results for synthetic phantom with randomly placed point targets. (top) phantom consists of 30 randomly placed point targets with minimum separation of 1 mm. (bottom) phantom consists of 110 randomly placed point targets with minimum separation of 0.25 mm.

## II. RESULTS

In this work we used field II ultrasound simulation software. The simulation experiment presented here includes a study on a phantom with randomly placed scatterers. In Figure 1. Ultrasound images reconstructed using CS were compared with conventional focused B-mode images.

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